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A Large Scale (N=400) Investigation of Gray Matter Differences in Schizophrenia Using Optimized Voxel-based Morphometry

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Abstract

Background—Many studies have employed voxel-based morphometry (VBM) of MRI images as an automated method of investigating cortical gray matter differences in schizophrenia. However, results from these studies vary widely, likely due to different methodological or statistical approaches.

Objective—To use VBM to investigate gray matter differences in schizophrenia in a sample significantly larger than any published to date, and to increase statistical power sufficiently to reveal differences missed in smaller analyses.

Methods—Magnetic resonance whole brain images were acquired from four geographic sites, all using the same model 1.5T scanner and software version, and combined to form a sample of 200 patients with both first episode and chronic schizophrenia and 200 healthy controls, matched for age, gender and scanner location. Gray matter concentration was assessed and compared using optimized VBM.

Results—Compared to the healthy controls, schizophrenia patients showed significantly less gray matter concentration in multiple cortical and subcortical regions, some previously unreported.

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Conclusions—Gray matter differences in schizophrenia are most comprehensively elucidated using a large, diverse and representative sample.

Keywords

Schizophrenia; Structural MRI; multi-site; voxel based morphometry; gray matter

1. Introduction

MRI studies of schizophrenia report approximately 2% less global gray matter (GM) volume in patients (Wright et al., 2000) and disproportionately less focal GM volume in many (perhaps especially heteromodal association cortex (HASC) regions (Baumann and Bogerts, 1999; Bucahanan et al., 2004; Falkai et al., 2001; Keshavan et al., 2003; Mesulam, 2004; Pearlson et al., 1996; Schlaepfer et al., 1994; Wright et al., 2000).

Lately, investigators have employed voxel-based morphometry (VBM; Ashburner et al., 2000), an efficient whole brain unbiased technique, to examine structural MRI differences. VBM provides automated measures of highly localized regions that may not be investigated in hypothesis-based studies that employ more labor-intensive region of interest (ROI) measures. VBM identifies regional differences in the concentration/volume of gray or white matter between groups, including GM alterations in schizophrenia versus healthy controls (Ananth et al., 2002; Gaser et al., 1999; Hulshoff Pol et al., 2002; Kubicki et al., 2002; Moorhead et al., 2004; Sigmundsson et al., 2001; Sowell et al., 2000; Suzuki et al., 2002; Wilke et al., 2001; Wright et al., 1999). These confirm and extend ROI studies (Gaser et al., 1999; Honea et al., 2005; Job et al., 2002) by increasing the anatomical range of volumetric comparisons. Schizophrenia samples exhibit lower GM concentrations in cingulate gyrus (Hulshoff Pol et al., 2002; Kubicki et al., 2002; Sigmundsson et al., 2001; Sowell et al., 2000), all frontal gyri (Gaser et al., 1999; Moorhead et al., 2004; Suzuki et al., 2002; Wilke et al., 2001), superior temporal gyrus (Gaser et al., 1999; Hulshoff Pol et al., 2002; Kubicki et al., 2002; Sigmundsson et al., 2001; Sowell et al., 2000; Suzuki et al., 2002; Wilke et al., 2001), medial temporal lobe (Hulshoff Pol et al., 2002; Sigmundsson et al., 2001; Suzuki et al., 2002; Wilke et al., 2001), insula (Hulshoff Pol et al., 2002; Kubicki et al., 2002; Sigmundsson et al., 2001; Wright et al., 1999) and thalamus (Ananth et al., 2002; Gaser et al., 1999; Hulshoff Pol et al., 2002; Sowell et al., 2000). Some VBM studies also demonstrate greater concentrations of GM among schizophrenia samples in the basal ganglia (Gaser et al., 1999; Kubicki et al., 2002; Wilke et al., 2001) and cerebellum (Kubicki et al., 2002; Suzuki et al., 2002), with the former perhaps attributable to first-generation antipsychotic treatment.

The statistical power of previous studies, however, has been relatively low, with most samples including fewer than 50 participants (Ananth et al., 2002; Kubicki et al., 2002; Wilke et al., 2001; Wright et al., 1999). These samples are large enough to reveal consistent fronto-temporal differences (Wright et al., 1999; Shenton et al., 2001), but differences in more anatomically variable regions, e.g. inferior parietal lobule, are reported less consistently. According to a recent meta-analysis of VBM studies (Mechelli et al., 2005), differences in the latter areas, though real, are inconsistently found due to the variations in size of smoothing kernels used across studies, the heterogeneity of schizophrenia itself, and failure of small samples to adequately represent the disease. Even though our study was not designed as a prospective multi-center study, similarities in acquisition parameters across the four different sites allowed us to pool data across scanners. By using VBM to investigate GM in a large and diverse schizophrenia sample, we hoped to increase statistical power sufficiently to reveal subtle

differences missed in smaller analyses. Also, by using a sample incorporating patients from varied backgrounds and areas, we aimed to increase generalizability of our results.

2. Methods and Materials

2.1. Subjects

We combined data from four separate studies conducted at Johns Hopkins University (JHU), the Maryland Psychiatric Research Center (MPRC), the Institute of Psychiatry, London, UK (IOP), and the Western Psychiatric Institute and Clinic at the University of Pittsburgh (WPIC). Samples were matched for age and gender within each site. The combined sample comprised 200 schizophrenia patients (78 females, mean age = 39.7, SD = 12.0, range 17–81) and 200 matched healthy controls (99 females, mean age = 40.0, SD = 14.8, range 16–79) and contained both first episode and chronic patients (see Table 1).

At each site, schizophrenia or schizoaffective disorder patients were diagnosed using the Structured Clinical Interview for DSM-III-R/DSM-IV (SCID; First et al., 1997; Spitzer et al., 1989), direct assessment, family informants, and past medical records. Healthy controls from the IOP, MPRC and WPIC samples were recruited from a pool of community volunteers; JHU controls were recruited using random-digit dialing as part of a community study (Schretlen et al., 2003). All control subjects were evaluated with the same structured interview as patients and excluded for a history of DSM-III-R/DSM-IV Axis I or Axis II disorder or major mental illness in first-degree relatives. Exclusion criteria for all samples included a history of overt brain disease, mental retardation, head injury with loss of consciousness over 60 minutes, or a diagnosis of substance abuse or dependence within the last 12 months.

2.2. MR imaging parameters

At all sites, whole brain MRIs were obtained on a 1.5T Signa GE scanner (GE Medical Systems, Milwaukee) in the coronal plane using a SPGR three-dimensional imaging sequence with the same software version. Between sites, almost every parameter was identical (35msec TR, 5msec TE, 45° flip angle, 1 excitation, 1.5mm slice thickness, 24cm field of view, and a matrix size of 256×256), except for IOP data, which were obtained using a 35° flip angle and a 20cm field of view.

2.3. Data Analysis

All images were visually inspected for orientation and movement artifacts, organized for preprocessing and analyzed using the SPM2 (http://www.fil.ion.ucl.ac.uk/spm/software/spm2/) software running in MATLAB 6.5.1 (The MathWorks, MA, USA).

2.3.1. Template Creation—Template creation utilized images from all 200 control subjects only. The control structural MRI scans were transformed to the same stereotactic space by registering each of the images to the ICBM 152 template (Montreal Neurological Institute). Normalized images were interpolated to voxel dimensions of 1.5mm³ and segmented into GM, white matter (WM) and cerebrospinal fluid (CSF). Images were then smoothed with an 8mm full-width half-maximum Gaussian kernel and averaged across subjects to create T1, gray, white and CSF templates. The templates were created using only healthy subjects to avoid confounding normalization with possible disease-related patients' data.

2.3.2. Optimized VBM—We employed the optimized VBM approach as detailed in Good et al 2001, using the above templates. To minimize mis-segmentation error, normalization was performed using the segmented GM and WM images. Original structural MRI images were segmented in native space and the resulting gray and white matter images then spatially

normalized to gray and white matter templates respectively to derive the optimized normalization parameters. These parameters were then applied to the whole-brain structural images in native space prior to a new segmentation (Good et al 2001; Mechelli et al., 2005).

We examined modulated and unmodulated voxel values in the segmented images. Modulation (Good et al., 2001) retains the absolute GM volume (GMV) post-normalization, whereas unmodulated data tests for regional differences in GM concentration (GMC; Good et al., 2001). Automated measures of whole brain tissue volumes for each subject were combined to obtain a measure of total intracranial volume (TIV).

2.4. Statistical Analyses

Comparisons were performed using an Analysis of Covariance (ANCOVA) model that included age, gender, site and TIV as covariates. We examined GMC differences bidirectionally for Controls versus Schizophrenia. The resulting set of voxels from each contrast represents a t-statistic map (SPM-t). SPM-t maps were thresholded for the main group comparison at p < 0.05 and corrected for multiple comparisons using the family wise error rate (FWE).

Coordinates of the most significantly different voxels were transformed from the MNI system to Talairach standard space (Talairach and Tournoux, 1998) using a MATLAB conversion program written by Matthew Brett (MRC Cognition and Brain Sciences Unit, England). Coordinates were then entered into the Talairach Daemon (Lancaster et al., 2000) to localize results.

To validate our study further, we investigated the main effects of site/location using only controls, by modeling only the 3 main (large) groups (JHU, WPIC and MPRC), excluding the smallest group (IOP) which contained significantly fewer subject numbers and used slightly different acquisition parameters. This analysis used an ANCOVA controlling for gender. An omnibus F-contrast examined any main effect of site. Additionally, multiple post-hoc t-tests (all combinations) were carried out and all resulting t-contrasts pooled in a null conjunction analysis at a threshold of p<0.05 FWE corrected for multiple comparisons, to reveal common gray matter differences between sites.

3. Results

3.1. Optimized GMC

In the whole sample, numerous regions showed significantly (p<0.05 FWE Corrected, t = 5.28) lower GMC in patients versus controls (Figure 1). Table 2 details relative volumes and Talairach coordinates of the significant areas. No region showed a significantly higher GMC in patients when corrected for multiple comparisons.

The whole 400-subject sample was divided by scanner location to examine differences within sub-groups. Groups were demographically matched across each site (Table 1). JHU subjects (133 SZ, 136 HC) comprised the majority of subjects, and accordingly displayed GMC differences similar to those found in the entire sample. Volumes and coordinates of regions showing significantly (p<0.001 FDR corrected, t = 3.84) lower GMC in JHU patients, relative to JHU healthy controls, are listed in Table 3. No region showed higher GMC in patients when corrected for multiple comparisons. Even when analyses were thresholded at the p<0.001 uncorrected level, in this large sample, we did not find increased GMC in any subcortical nuclei. Clusters found in the JHU sample that were also found in the complete sample were all smaller in volume.

Comparisons were also contrasted within the smaller samples from each site. Results from the MPRC scans were detailed in Giuliani, et al 2005. MPRC schizophrenia patients demonstrated (p<0.001 FDR corrected, t = 3.84) lower GMC in several regions as detailed in table 3). No region showed a significantly higher GMC in patients in the MPRC sample at this threshold. In the WPIC sample, at p<0.001 FDR corrected, patients had lower GMC in multiple cortical regions (See Table 3). No regions contained significantly higher GMC in schizophrenia patients. Due to the small number of images collected at the IOP (N=8, 11), the data were not analyzed individually.

3.2. Optimized GMV

In a whole sample voxel-by-voxel contrast, corrected for multiple comparisons, no regions showed (p<0.05, FWE Corrected) smaller GMV in schizophrenia.

As GMV results replicated the GMC pattern at lesser statistical significance, we investigated the impact of the additional modulation step. By calculating the mean of both groups using both optimized VBM methods (Figure 2), it is apparent that both methods reveal the same pattern of less GM in patients in the frontal, temporal, and subcortical/limbic regions, and more GM in the occipital and bordering ventricular regions. Calculating the standard deviation by group demonstrated that the images from patients with schizophrenia had more variance than healthy controls.

3.3. Main effect of Site

Examining main effect of site in controls revealed GMC differences in a small number of brain regions; however this location and pattern of GM difference (Figure 3 - shown in green) had minimal spatial overlap with our main effect of GM reductions in patients (Figure 3 - shown in orange), emphasizing that main effect of site had little impact on the latter findings. Table 2 also illustrates an approximate quantitative estimate of percentage overlap in suprathreshold voxels in these areas. Additionally, the evaluation of GMC differences across sites using a conjunction analysis (Etgen et al., 2005) revealed no significant voxels at the p<0.05 FWE corrected threshold.

Multiple brain imaging studies indicate widespread gray matter volume abnormalities in schizophrenia. Since 1999, almost 30 studies surveying the whole brain using VBM in schizophrenia; have found less GM in fronto-temporal regions, as summarized in Table 4. However, even with such an automatic method, studies disagree. The sample size of 200 patients and 200 matched controls makes the current VBM study of GM changes in schizophrenia the largest to date.

Our results complement previous ROI and VBM research in documenting less frontal, parietal, temporal, and sub-cortical GM reductions in schizophrenia. The main effects contrast found lower GMC in all published regions, plus areas including the superior parietal lobule, caudate, rectal gyrus, and transverse temporal gyrus. The only region previously documented as containing less GMV in schizophrenia undetected in our analyses was hippocampus, possibly because the peak difference in medial temporal lobe lies in the parahippocampal gyrus, only extending into the hippocampus proper at lower thresholds. Furthermore, GM changes in smaller sub-cortical structures, e.g. hippocampus, are harder to detect using VBM due to inherent problems in normalization and smoothing (Bookstein, 2001; McIntosh et al., 2004).

The most notable difference in our findings compared to previous studies is the larger number of regions we characterized as containing less GM in schizophrenia. This is not explained by differences in significance thresholds, as our p-value of p<0.05 corrected for multiple comparisons (FWE) is very stringent. One explanation is sample size. Another is

methodological differences in the implementation of VBM. We addressed the first question by amassing the largest number of patients and matched controls to date. Increasing subject numbers also increases statistical power. The next largest VBM study, performed by Hulshoff Pol et al., 2002, at a threshold of p<0.05 corrected for multiple comparisons (|t| > 5.0), schizophrenia patients had less GM in several temporal lobe areas, but few additional significant findings. In contrast to our data, however, that study did not capture GM differences in several critical areas such as the superior, middle, inferior frontal gyri, parahippocampus, amygdala and inferior parietal lobule, (See Table 4).

4. Discussion

4.1. Methodology

Our main methodological strength is the use of optimized VBM, namely the normalization of GM segments to a study-specific template. This ensures the reflection of GM distribution found within the study cohort, accounts for any data inhomogeneities due to scanner differences used, and ensures a minimal warping is required for coregistration. Also, normalization of the GM segments to the study-specific GM template reduces erroneous inclusion of missegmented non-brain voxels.

As our data was collected at four different sites, we tested robustly for scanner differences by: 1) Using a study-specific template to minimize effects of using data from four sites. 2) Accounting for confounding variables such as gender, location, age, and total intracranial volume. 3) Accessing a main effect of site to look at any GM differences that existed across scanners. 4) Using conjunction analysis to verify homogeneity of GM differences across sites. The decision to use only the healthy subjects' images to create the templates was supported by an ad hoc analysis of the data using a template from all 400 subjects, where results did not differ significantly from those reported. The normalization procedures, although highly reliable, render the VBM process less sensitive to group differences in shape or gray-white matter differentiation than previous ROI methods, and may misregister anatomical structures (Ashburner and Friston, 2001; Bookstein, 2001). The removal of global size differences in the normalization process is a caveat in all VBM studies, especially if brain atrophy is documented.

Several studies (Keller et al., 2004) have explored modulation to extend and possibly improve optimized VBM results. Comparing modulated and non-modulated VBM results, Keller et al. (2004) found more regions of GM loss using VBM of GMV than GMC, concluding that optimized VBM of GMV was more accurate to assess differences in regional brain volume. We found similar areas of lower GMV in patients, albeit less significant than the GMC results (Figure 2), due to increased within-group variance of patients' GM volumes. The multiplication by Jacobian determinants accounts for varied GM partitions and decreases statistical power.

4.2. This sample

The results from the whole sample and the individual site subsamples resembled each other except in parietal, occipital and limbic sub-regions, which we discuss by site. As two thirds of the main sample consisted of scans collected at JHU, a contrast of only those controls and patients should elicit GM differences in the majority of the same regions as the main effects analyses. Schizophrenia patients demonstrated significantly lower GMC in all areas seen in the main effects analysis with few exceptions discussed here (Table 3). All regions exhibiting differences in both the main effects and JHU samples were smaller in volume in the latter, consistent with our hypothesis that these regions would be less significant due to the smaller sample size of the JHU group.

were not very significant.

It is impossible to tell whether sites with only chronic patients (MPRC) or only first episode unmedicated patients (WPIC) show differences due to illness stage or medication effects, or both. Cingulate gyrus, thalamus, middle temporal gyrus and transverse temporal gyrus differed from controls in chronic, but not first episode patients, consistent with the progression of GM changes seen in first episode patients followed longitudinally (Nakamura et al., 2007). An additional caveat of the study is the influence of former substance dependence (greater than 12 months) on any gray matter volume changes.

While the purpose of this study was not to examine between-site differences, we saw similar patterns of less GMC in schizophrenia within each of the sub-samples. The location of GMC differences varied slightly by site, as shown in Table 3, but all three sub-samples demonstrate significantly lower GMC in patients in most HASC regions. The other difference between samples is that of statistical significance, due to different sample sizes. The additive properties of these separate samples suggest benefit in combining images from several scanners. By using groups from Baltimore, Pittsburgh and London we account for unique subject-selection, geographical, and scanner-related variation. Interestingly, data from two sites within the city of Baltimore yielded different results, demonstrating that even combining geographically similar samples results in a more statistically powerful and generalizable sample.

4.3. Conclusion

We present the largest VBM study to date investigating GM in schizophrenia. By increasing subject numbers and using optimized VBM methods, we observed more and larger regions containing less GMC in schizophrenia than prior published studies. Also, we demonstrated that modulation of VBM results, converting GMC to GMV, did not improve our data. Regardless, these results suggest that VBM analyses of schizophrenia are greatly enhanced by using large, representative sample.

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Figure 1.

Main effect group map with lower GMC (FWE corrected p<0.05, t=5.28) in schizophrenia patients relative to healthy controls.



Figure 2.

Direct comparison of GMV and GMC results from the control > patient contrast. Areas in red contain more GM in control subjects, areas in blue contain more GM in schizophrenia patients. One slice from each GMC, GMV, mean and standard error of the mean (SEM) displayed. The GMC contrast has a higher mean and lower SEM than the GMV contrast, which corresponds to decreased statistical power of the latter.



Figure 3.

Simultaneous overlay of GM concentration differences between the three major scanner sites (Displayed in green at p< 0.05, F = 18.3, FWE corrected for multiple comparisons.) and diagnosis (Displayed in orange at p<0.05 FWE corrected).

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						Table 1					
	D	Demographic dat	ta of particips	ants incl	luded in the stuc	dy, by scanne	r location.				
	*	(1=male, 2=fem	iale)								
Site		HEALTHY			SCHIZOPHREN	IIA		Age		Sex	
	Z	Age (Mean ± Stdev)	Sex (M/F)	Z	Age (Mean ± Stdev)	Sex (M/F)	Diagnosis (First Episode/Chronic)	t-score	p value	Chi square	p value
UHL	136	41.835 ± 16.22	61/69	133	41.579 ± 12.60	70/63	16(drug free)/117	0.14	0.88	0.18	0.67
MPRC	34	42.54 ± 6.88	17/17	34	41.318 ± 5.33	24/10	$\tilde{0}/34$	0.81	0.41	2.21	0.14
IOP	6	35.667 ± 7.26	4/5	Π	41.091 ± 8.80	4/7	0/11	-1.47	0.15	0.13	0.71
WPIC	21	26.238 ± 7.49	13/8	22	25.091 ± 7.01	14/8	22 (treatment naïve)/0	0.51	0.3	0.01	0.9
TOTAL	200	40.04 ± 14.77	101/99	200	39.694 ± 12.06	112/88	38/162	0.25	0.39	1.01	0.31

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Table 2Areas with lower GMC in patients relative to controls: (FWE corrected p<0.05, t= 5.28)</td>

Whole Sample, GMC: A summary of areas detected in the main effects analysis by diagnosis (controls > patients) along with their Talairach coordinates, volume and maximum t-value and its coordinate at a corrected p<0.05 (FWE, t=5.28). For all tables, each volume listed is the size of the cluster of contiguous voxels above a given threshold in each area. Also provided are the extent of GMC differences

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overlap bet	tween main effect of diagnosis and site.						
Regions	Brodmann Areas	L (Vol CC)	$\operatorname{Max} T(\mathbf{x}, \mathbf{y}, \mathbf{z})$	R (Vol CC)	Max T (x, y, z)	Percentage	Overlap
1						Γ	R
Inferior Frontal Gvrus	47, 45, 44, 46, 11, 13	8.2	8.3(-42,19,-7)	10.6	7.6(46, 18, 2)	3.66	1.89
Medial Frontal Gyrus [*]	10, 9, 11, 32, 6, 8	6.8	7.5(-3,60,-4)	8.5	7.4(3,60,-4)	14.70	8.23
Insula	47,13, 22, 40	6.9	7.9(-42,17,-2)	6.7	7.3(43,16,2)		
Superior Temporal Gyrus	22, 38, 13, 42, 41	4.8	7.4(-46,13,-7)	5.5	7.5(49,4,1)	6.25	1.82
Middle Frontal Gyrus [*]	11, 10, 46, 9, 6, 8	9	7.0(-28,31,-17)	4.1	6.5(50,23,22)	6.67	9.76
Superior Frontal Gvrus	10, 9, 8, 6	5.8	7.6(-3,61,-2)	2	7.4(3,61,-2)	25.86	60
Anterior Cingulate	10, 32, 25, 42, 24	2.8	7.1(-3,55,-1)	2.6	7.3(6,54,-1)	17.86	15.38
Precentral Gyrus	44,6, 13, 43, 42	2.5	7.2(-50,11,6)	2.1	7.5(50,18,6)		
Postcentral Gyrus	43, 2, 1, 3, 40	0.5	6.0(-53, -18, 15)	1.8	6.5(52,-17,17)		
Cingulate Gvrus	32, 24	1.4	6.2(-6, 30, 26)	0.6	5.9(7,20,27)	21.43	16.67
Transverse Temporal Gyrus	41,42	0.6	6.1(-50,-20,13)	0.6	6.1(48,-17,13)		
Thalamus	Medial Dorsal Nucleus, Pulvinar, Mammillary	0	NS	0.9	6.1(6, -19, 4)		
	Body						
Caudate	Caudate Head	0.1	5.6(-4.9,0)	0.4	6.1(4,9,0)		
Orbital Gyrus	11	0.3	6.5(-4,46,-19)	0.1	6.1(3,43,-19)		
Posterior Cingulate	23	0.4	5.8(-10, -53, 12)	0	NS		
Rectal Gyrus	11	0.1	6.3(-4,37,-20)	0.1	6.1(1,37,-20)		
Subcallosal Gyrus	25	0	NS	0.1	5.5(3,7,-14)		
Middle Temporal Gyrus	21	0.1	5.3(-52,0,-24)	0.1	5.4(62,-11,-11)		
Inferior Parietal Lobule	39	0	NS	0.1	5.5(65,-22,26)		
Inferior Temporal Gyrus	19	0.1	5.4(-52,-61,-2)	0	NS		
Uncus	28	0.1	5.4(-24,7,-26)	0	NS		
Middle Occipital Gyrus	19	0.1	5.3(-52,-61,-4)	0	NS		
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Regions where GMC differences due to effect of site and diagnosis both overlap each other.

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Table 3

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 $\begin{array}{c} 4.5(-10,-55,11)\\ 4.9(-52,-61,-2)\\ 5.1(-55,-1,-23)\\ 5.1(-55,-45,23)\\ 4.4(-53,-45,23)\\ 5.1(-52,-61,-4)\\ 4.2(-19,-31,-10)\\ 4.2(-19,-31,-10)\\ 4.2(-19,-31,-10)\\ 4.2(-53,-46,20)\\ 4.3(-53,-46,20)\\ 4.3(-53,-46,20)\end{array}$

0.3 0.1 0.1 0.2 0.1 0.1

0.8 2 1.6 0.2 0.4 0.4 0.4

2.5(58,-22,-30)

3.4(-56,-26,-31)

0

0.6

2.6(12,-81,7)

2.7(-21,-62,20)

0.1

0.1

4.2(21,8,-24)

4.1(-15,6,-19)

0.6

0.1

4.7(12,-63,45) 4.4(24,-70,-4) 4.4(28,-6,-35) 4.2(24,-25,-1)

4.1(-10,-48,40) 4.1(-30,-57,-2) 4.7(-27,9,-29) 5.8(-1,57,1)

1.4 0.3 0.6 0.1

0.3 0.1 0.5 0.1

Fugförm Gyrus Suppamarginal Gyrus Suppallosal Gyrus Par<u>a</u>hippocampal Gyrus

5.0(4,8,-14) 4.0(10,-1,-21) 3.9(61,-11,-25)

4.8(-4,7,-10) 3.9(-10,2,-20)

0.8 0

<mark>0.8</mark> 0.1

N.S.

0

N.S. 4.1(52,-48,25) N.S. 4.2(25,-28,-4)

By Site,	GMC: A	summai	ry of areas detected	d in the JHU, MI	PRC and	I WPIC	sub-sample ana	lyses by diagnosi	s (contre	$ds > p_{i}$	atients) along	
with thei	r Talaira	ich coord	linates, volume ar	id maximum t-va	alue and	its coo	rdinate at a corr	ected p<0.001 (F	DR, $t=3$.84).		
			JHU SUBJECTS				MPRC SUBJECTS				WPIC SUBJECTS	
Rrain Region	10 V OI	(20) B	I.	x,y,z) R) IO ((() S	I.	(X,Y,Z) R		ے <mark>م</mark>	I.	k,y,z) R
Inferior Frontal Gyrus	12.6	15.9	6.8(-9.40,-16)	6.4(30,27,-15)	2.6	2.8	4.9(-43.9.29)	5.1(33,20,-16)	1.8	3.4	3.1(-52,19,-3)	3.3(50,25,11)
Middle Frontal Gyrus	9.6	9.4	5.7(-24,27,-18)	6.1(30,33,-13)	1.3	0.9	4.4(-43,15,28)	4.4(28,34,43)	2.7	0.9	3.7(-58,52,-13)	3.1(27,38,-21)
Precentral Gyrus	4	2.3	5.2(-48,2,48)	5.0(49.18,6)	0.7	0.6	4.7(-50,7,13)	4.6(53,9,4)	1.7	0.3	3.0(-53,-5,24)	2.8(50,16,9)
Insula	4.3	4.6	5.3(-39,16,-1)	5.0(40, 19, 2)	1.4	1	4.9(-42,2,-11)	4.2(40,11,-9)	2.7	1.7	3.2(-33,13,8)	3.3(36,-12,13)
Superior Temporal Gyrus	7.2	5.4	5.6(-45,15,-11)	5.2(48, 14, -7)	1.7	2.8	5.2(-42,-1,-14)	4.8(53,6,2)	0.8	0	2.7(-64,-23,12)	N.S.
Medial Frontal Gyrus	12.5	12.4	7.0(-7,43,-16)	6.1(7, 49, -4)	2.4	4.5	5.3(-6,62,-12)	6.5(7,64,0)	0.9	1.7	4.4(-7,70,-5)	3.5(4,72,-9)
Superior Frontal Gyrus	7.4	4.1	5.6(-18, 39, 30)	5.8(6.54, -1)	3.2	3.9	5.2(-6.62, -9)	6.3(7,62,-3)	4	3.4	4.9(-12,73,-2)	3.3(25,40,-23)
Claustrum	0.5	0.5	4.7(-34,15,2)	4.5(36, -8, 11)					1.5	0.7	3.3(-33,-14,15)	3.2(34,-15,12)
Anterior Cingulate	4.2	2.1	5.9(-3.54,-1)	6.0(6.51, -1)	0.8		5.0(-4.5,-8)	4.9(4.5, -7)	0.4	0.6	2.9(-1,13,-1)	2.9(1,13,-1)
Postcentral Gyrus	1.1	2.2	4.4(-53,-17,15)	5.0(53, -18, 19)	0	0.2	N.S.	4.1(64, -19, 31)	0.2	0.3	2.7(-53, -8, 20)	2.7(25,-43,70)
Hygothal./Substantia Nigra					0.2	0.8	4.8(-6.8, -8)	5.0(6,5,-10)				
Recial Gyrus	-1	0.6	5.9(-6,37,-20)	5.3(0,37,-20)								
Cinculate Gyrus	3.4	0.9	5.5(-12, -4, 40)	4.3(10, -40, 37)	0.2	1.1	4.0(-9, -17, 35)	5.1(12, -13, 37)				
Orbital Gyrus	0.9	0.4	6.5(-6,43,-19)	5.4(0,43,-19)					0	0.1	N.S.	2.8(22,38,-25)
Thatamus	0.1	2.1	4.0(-9, -14, 9)	4.7(13, -18, 9)	0.8	1.2	4.8(-1, -19, 8)	4.9(0, -17, 4)				
Transverse	0.9	0.4	4.4(-50, -20, 12)	4.3(58,-12,14)	0	0.1	N.S.	4.0(55, -20, 12)				
Teraporal Gyrus												
Cattiate					-1	1.5	4.9(-4, 8, -5)	4.8(4.9, -4)	0.5	0.6	2.9(-3,15,-1)	2.9(3,15,1)
Posterior Cingulate	0.8	0	4.5(-10,-55,11)	N.S.					0.3	0.1	2.8(-18, -55, 17)	2.7(24,-54,18)
Inferior Temporal Gyrus	2	0.3	4.9(-52,-61,-2)	4.2(31, -6, -35)	0	0.5	4.1(-43, -4, -16)	4.5(64,-13,-23)	0.5	0.5	3.4(-55,-26,-34)	3.2(56,-25,-33)
Middle Temporal Gyrus	1.6	0.7	5.1(-55,-1,-23)	4.5(62, -11, -11)	0	0	4.0(-43.1, -19)	3.9(65, -15, -14)				
Inférior Parietal Lobule	0.2	0.1	4.4(-53,-45,23)	4.3(56, -19, 22)					0	0.1	N.S.	2.5(65,-40,45)
Middle Occipital Gyrus	0.3	0	5.1(-52,-61,-4)	N.S.								
Amrgdala	0.6	0.2	4.2(-19, -31, -10)	4.2(25,-28,-4)								
i												

Predmeus Lingual Gyrus Lates Geniculum Body 1 liud 6 6 eniculum Body

Table 4

Summary of regions with significantly less GM in schizophrenia patients than healthy controls by scanner and study (1 = current study, all subjects; 2 = current study, JHU subsample; 3 = current study, MPRC subsample; 4 = Moorhead, 2004; 5 = McIntosh, 2004; 6 = Ananth, 2003; 7 = Giuliani, 2004; 8 = Suzuki, 2002; 9 = Palliere-Marinot, 2001; 10 = Hulshoff Pol, 2001; 11 = Kubicki, 2002; 12 = Wilke, 2001; 13 = Antonova, 2003; 14 = Wright, 1999; 15 = Job, 2002; 16 = Gaser, 1999; 17 = WPIC subsample)

	1 /	
Brain Region	Current study site	Prior Study
Superior Frontal Gyrus	1,2,3,17	4,6,7,8,16
Middle Frontal Gyrus	1,2,3,17	5,7,8,11,14,16
Medial Frontal Gyrus	1,2,3,17	6,7,9,12,15
Inferior Frontal Gyrus	1,2,3,17	5,6,7,8,12
Orbital Gyrus	1,2,17	6,10,12
Rectal Gyrus	1,2	
Precentral Gyrus	1,2,3,17	6,7,9,13,16
Subcallosal Gyrus	1,3	7
Postcentral Gyrus	1,2,3,17	6,7,15
Insula	1,2,3,17	7,9,10,11,12,14
Superior Temporal Gyrus	1,2,3,17	4,7,8,10,11,12,13,14,16
Middle Temporal Gyrus	1,2,3	7,10,12,13,15
Inferior Temporal Gyrus	1,2,3,17	4,6,7,10,13
Transverse Temporal Gyrus	1,2,3	7
Parahippocampal Gyrus	1,3	4,5,7,9,13,15
Hippocampus		8,10,11
Amygdala	1,2	10,14,15
Uncus	2,3	7,15
Anterior Cingulate	1,2,3,17	7,8,9,11,15
Posterior Cingulate	1,2,17	7,10
Superior Parietal Lobule	1	, ,
Inferior Parietal Lobule	1,2,17	6,11
Supramarginal Gyrus	1,2	,
Middle Occipital Gyrus	1,2	6
Fusiform Gyrus	1,2,3,17	6,7,9
Lingual Gyrus	1,2	16
Precuneus	1,2	10
Cuneus	1	4
Caudate	1,3,17	7
Thalamus	1,2,3	5,6,7,10,16
Claustrum	1,2,3,17	7
Lateral Geniculum Body	2,3	7
Hypothalamus	1,3	7